

ORIGINAL**Mineral to matrix ratio determines biomaterial and biomechanical properties of rat femur -application of Fourier transform infrared spectroscopy-**

Shinjiro Takata¹, Hiroshi Yonezu², Akira Shibata³, Tetsuya Enishi¹, Nori Sato¹, Mitsuhiro Takahashi⁴, Shigetaka Nakao¹, Koji Komatsu¹, and Natsuo Yasui^{1,4}

¹Division of Rehabilitation, Tokushima University Hospital, Tokushima, Japan ; ²Department of Orthopedic Surgery, Mitoyo General Hospital, Kagawa, Japan ; ³Faculty of Pharmaceutical Science, Yasuda Women's University, Hiroshima, Japan ; and ⁴Department of Orthopedics, Institute of Health Biosciences, the University of Tokushima Graduate School, Tokushima, Japan

Abstract : We studied the changes of biomaterial and biomechanical properties of the rat femur during development. Thirty male Wistar rats were allocated to 6 groups : aged 6 weeks (n=5), 9 weeks (n=5), 12 weeks (n=5), 15 weeks (n=5), 24 weeks (n=5), and 36 weeks (n=5). The mineral to matrix ratio (M/M ratio) of rat femur by Fourier transform infrared spectroscopy was 0.97 ± 0.10 at the age of 6 weeks, and reached the maximum of 1.52 ± 0.17 at the age of 36 weeks. Total bone mineral density (BMD) by peripheral quantitative computed tomography of the femoral shaft aged 6 weeks was $479.1 \pm 58.7 \text{ mg/cm}^3$, and reached the maximum of $1022.2 \pm 42.3 \text{ mg/cm}^3$ at the age of 36 weeks. The ultimate load to failure of the femur of the rat aged 6 weeks by the three-point bending test was $29.6 \pm 6.1 \text{ N}$. At the age of 36 weeks, the ultimate load to failure of the rat femur increased to the maximum of $283.5 \pm 14.7 \text{ N}$. The results showed that the M/M ratio increased with development as total BMD and bone strength increased. The results suggest that the M/M ratio is one of the determinants of the biomaterial and biomechanical properties of bone. *J. Med. Invest.* 58 : 197-202, August, 2011

Keywords : Fourier transform infrared spectroscopy, bone quality, peripheral quantitative computed tomography, three-point bending test

INTRODUCTION

The changes of biomaterial and biomechanical properties of bone during development and aging affect bone strength. Bone strength is determined by both bone quantity and quality. Bone quantity, including bone mineral density (BMD) and bone

mineral content (BMC), accounts for approximately 75-80% of the variance in bone strength (1). Bone quality is assessed by the architecture, turnover, damage of accumulation (e.g., microfractures), and mineralization of bone (2). The three-dimensional trabecular microarchitecture by micro-computed tomography (μCT) is one of the determinants of bone strength, apart from the BMD or BMC. Principally, μCT is principally applicable *in vitro* (3, 4). Fourier transform infrared (FTIR) spectroscopy allows us to examine the molecular structure and conformation of biological macromolecules because it measures the absorption energy which produces an increase

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Address correspondence and reprint requests to Shinjiro Takata, MD, PhD, Division of Rehabilitation, Tokushima University Hospital, 2-50-1, Kuramoto-cho, Tokushima 770-8503, Japan and Fax : +81-88-633-0178.

in the vibrational or rotational energy of atoms or groups of atoms within the molecule (4). Evaluation of bone mineralization is calculated the mineral to matrix ratio (M/M ratio) by FTIR (5-12). Biomechanical parameters of bone were made with three-point bending test according to the method of Molster *et al.* (13). Stiffness and ultimate load to failure of bone by three-point bending test were determined from a load-deflection curve (5).

The purpose of this study was to show changes in the M/M ratio of rat femur during development using FTIR spectroscopy. The results showed that the M/M ratio is an important determinant of the biomaterial and biomechanical properties of bone.

MATERIALS AND METHODS

Experimental Animals

All experimental procedures were approved by the local animal protection and ethics committee.

Thirty male growing Wistar rats were allocated to 6 groups: aged 6 weeks (n=5), 9 weeks (n=5), 12 weeks (n=5), 15 weeks (n=5), 24 weeks (n=5), and 36 weeks (n=5). The rats were euthanized by intraperitoneal injection of an overdose of sodium pentobarbital. Bilateral femora were removed to perform FTIR spectroscopy, peripheral quantitative computed tomography (pQCT), and the three-point bending test.

BIOMATERIAL PROPERTIES

1. Fourier Transform Infrared (FTIR) Spectroscopy

Femora were excised and the soft tissue, periosteum, and bone marrow were immediately removed. The midshaft of the diaphysis was frozen in liquid nitrogen and lyophilized for 48 hours to remove all water and then ground in liquid nitrogen. Infrared spectra were recorded by an FTIR spectrometer (FTIR-1720; Perkin-Elmer, Norwalk, USA) equipped with a triglycine sulfate detector with KBr windows. The samples were examined by the KBr technique (4).

A typical FTIR spectrum of the rat femur is shown in Figure 1. Peak positions near 1020 cm^{-1} and 1650 cm^{-1} were assigned to the phosphate stretching vibration of apatites and the amide I stretching vibration of the bone organic matrix, respectively (5). The spectral resolution was 4 cm^{-1} . The abscissa range was 900-1800 cm^{-1} , covering the phosphate

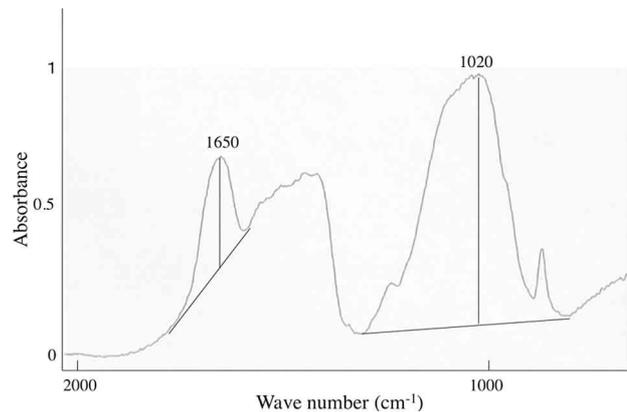


Figure 1. Fourier transform infrared spectroscopy (FTIR) spectra of rat femur.

Peak positions near 1020 cm^{-1} and 1650 cm^{-1} were assigned to the phosphate stretching vibration of apatites and the amide I stretching vibration of the bone organic matrix. The mineral to matrix ratio (M/M ratio) was calculated from the ratio of the absorbance of the phosphate band at 1020 cm^{-1} to the amide I band at 1650 cm^{-1} .

band and the amide I band. Data were Fourier transformed and averaged after 50 scans. The mineral/matrix ratio was calculated from the ratio of the absorbance of the phosphate band at 1020 cm^{-1} to the amide I band at 1650 cm^{-1} .

2. Peripheral Quantitative Computed Tomography (pQCT)

Bone mineral density (BMD), bone mineral content (BMC), bone area, periosteal and endosteal circumferences were measured by pQCT (XCT-960A; Norland/Stratec, Fort Atkinson/Pforzheim, USA/Germany). Measurements were taken using 1-mm-thick slices from the middle of the femoral shaft (diaphysis). Total BMD, cortical BMD, cancellous BMD, total BMC, cortical BMC, and cancellous BMC were measured.

Measurements of Bone Strength (Three-Point Bending Test)

The rat femurs were subjected to the three-point bending test. Measurements were conducted with a bone strength tester (Model MZ-500S; Marto, Tokyo, Japan) according to the method of Molster *et al.* (13). Each femur was positioned with the flexor surface side up on the top of two metal supports located at a distance of 13 mm in the tester, and the bending force was applied midway at the rate of 10 mm/min until fracture occurred. Bone strength was determined from a load-deflection curve.

STATISTICS

Results were expressed as the mean ± standard deviation (S.D.). One-way analysis of variance (ANOVA) was used to evaluate the significance of differences among the four groups. When ANOVA indicated significant differences among the six groups, the differences were evaluated using Fisher's protected least significant difference (PLSD). Correlations of M/M ratio with other biomechanical parameters including total BMD, periosteal and endosteal circumferences of femoral shaft, ultimate load to failure, and stiffness were assessed using linear regression analysis. A $p < 0.05$ value was considered significant.

RESULTS

Mineral/Matrix Ratio (M/M ratio) (Fig. 2)

The M/M ratio of rat femurs increased with development, being 0.97 ± 0.10 at the age of 6 weeks and rising to the maximum of 1.52 ± 0.17 at 36 weeks.

The M/M ratio exceeded 1.0 between the ages of 6 and 9 weeks, indicating that the relative amount of minerals exceeds that of matrix content. The increase rate of the M/M ratio was greatest between the ages of 6 and 9 weeks.

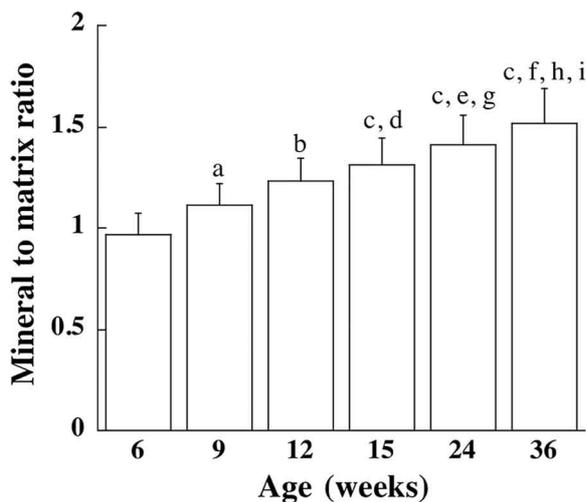
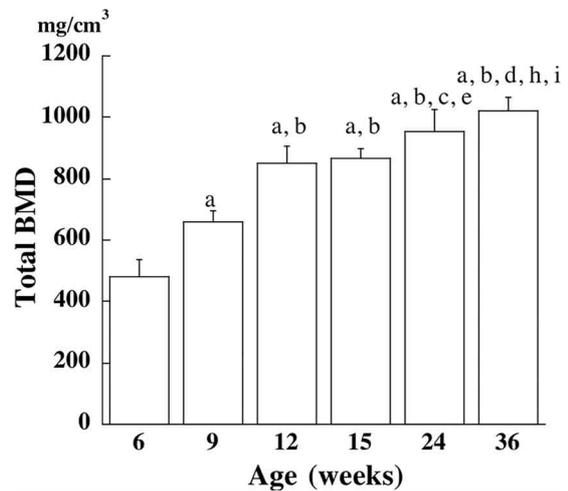


Figure 2. Mineral to matrix ratio (M/M ratio) of rat femur. M/M ratio of rat femur increased with development. M/M ratio exceeded 1.0 between the ages of 6 and 9 weeks. The increase rate of the M/M ratio between the ages of 6 and 9 weeks was greatest of all ages. aP=0.0235 vs. 6-week group, bP=0.0010 vs. 6-week group, cP<0.0001 vs. 6-week group, dP=0.0107 vs. 9-week group, eP=0.0004 vs. 9-week group, fP<0.0001 vs. 9-week group, gP=0.0232 vs. 12-week group, hP=0.0004 vs. 12-week group, iP=0.0071 vs. 15-week group

Bone mineral density (BMD), periosteal and endosteal circumferences (Fig. 3A-C)

The total BMD consists of cortical and cancellous BMD. The total BMD of the femoral shaft of

A



B

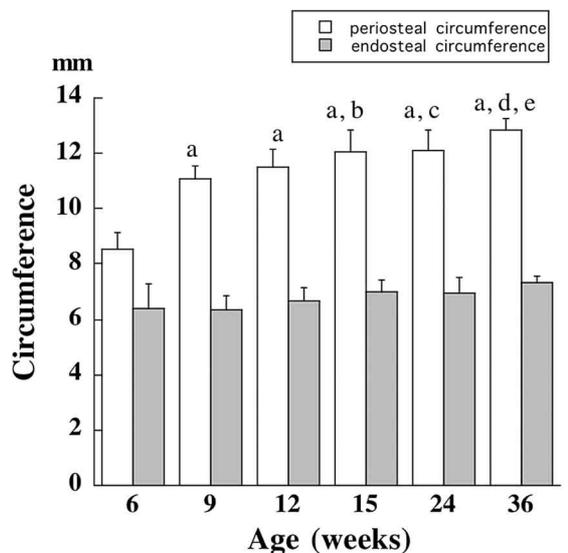


Figure 3A, B. BMD, periosteal and endosteal circumferences. Total BMD of rat femoral shaft increased during development and reached the maximum at the age of 36 weeks (A). Total BMD consists of cortical and cancellous BMD. Total BMD of the femoral shaft increased with development. The increase rate of total BMD was greatest between the ages of 6 and 9 weeks. aP<0.0001 vs. 6-week group, bP<0.0001 vs. 9-week group, cP=0.0030 vs. 12-week group, dP<0.0001 vs. 12-week group, eP=0.0110 vs. 15-week group, hP<0.0001 vs. 15-week group, iP=0.0496 vs. 24-week group. Periosteal circumference of femoral shaft increased during development, whereas there were no significant differences in endosteal circumference during development (B). Both periosteal and endosteal circumferences increased with development. The increase rate of periosteal circumference was greatest at between 6 and 9 weeks of age. aP<0.0001 vs. 6-week group, bP=0.0200 vs. 9-week group, cP=0.0166 vs. 9-week group, dP=0.0001 vs. 9-week group, eP=0.0022 vs. 12-week group

the rat aged 6 weeks was $479.1 \pm 58.7 \text{ mg/cm}^3$, and increased from 3 to 36 weeks (Fig. 3A). At the age of 36 weeks, this value reached to the maximum of $1022.2 \pm 42.3 \text{ mg/cm}^3$. The increase rate of total BMD was greatest between the ages of 6 and 9 weeks.

The periosteal circumference of the femoral shaft increased with development (Fig. 3B). This value at the age of 6 weeks was $8.6 \pm 0.6 \text{ mm}$. At the age of 36 weeks, this value rose to the maximum of $12.9 \pm 0.4 \text{ mm}$. The increase rate of the periosteal circumference was greatest between 6 and 9 weeks of age. The increase rate of the periosteal circumference of the femoral shaft was greatest between the ages of 6 and 9 weeks. The endosteal circumference of the femoral shaft also increased with development, being 6.4 ± 0.8 at the age of 6 weeks and increasing to the maximum of $7.3 \pm 0.2 \text{ mm}$ at the age of 36 weeks.

Bone strength and stiffness by three-point bending test (Fig. 4)

Bone strength, the ultimate load to failure of the femoral shaft of rats increased with development

(Fig. 4A). The bone strength of the femur of a rat aged 6 weeks was $29.6 \pm 6.1 \text{ N}$, which increased to the maximum of $283.5 \pm 14.7 \text{ N}$ at the age of 36 weeks. The increase rate of bone strength was greatest between the ages of 6 and 9 weeks.

The stiffness of the rat femur increased with development (Fig. 4B), being $44.6 \pm 7.9 \text{ N/mm}$ at the age of 6 weeks and reaching the maximum of $509.2 \pm 59.0 \text{ N/mm}$ at the age of 36 weeks. The increase rate of stiffness was greatest between the ages of 6 and 9 weeks.

Femoral length and body weight (Fig. 5A, B)

The femoral length in rats aged 6 weeks was $27.4 \pm 0.7 \text{ mm}$ (Fig. 5A), reaching $43.6 \pm 1.0 \text{ mm}$ at the age of 36 weeks. The increase rate of the femoral length was greatest between the ages of 6 and 9 weeks.

The body weight of rats aged 6 weeks was $159.0 \pm 4.2 \text{ g}$ (Fig. 5B), increased with development and reached the maximum of $598.0 \pm 153.5 \text{ g}$ at the age of 36 weeks. The increase rate of body weight was greatest between the ages of 6 and 9 weeks.

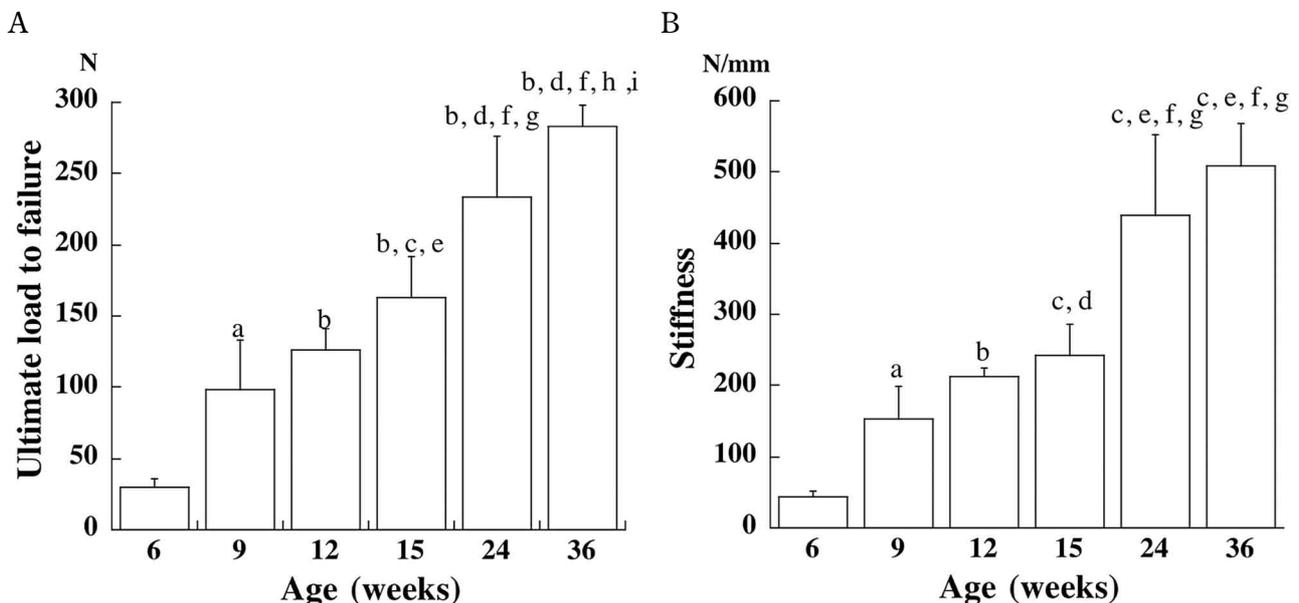


Figure 4A, B. Bone strength by three-point bending test.

Ultimate load to failure of femoral shaft of rat increased with development (A). The ultimate load to failure of femoral shaft increased during development. These increase rates of bone strength and stiffness were greatest between the ages of 6 and 9 weeks.

aP=0.0005 vs. 6-week group, bP<0.0001 vs. 6-week group, cP=0.0008 vs. 9-week group, dP<0.0001 vs. 9-week group, eP=0.0390 vs. 12-week group, fP<0.0001 vs. 12-week group, gP=0.0004 vs. 15-week group, hP<0.0001 vs. 15-week group, iP=0.0069 vs. 24-week group

Stiffness of femoral shaft of rat increased with development (B). The stiffness of the rat femur increased during development. These increase rates of bone strength and stiffness were greatest between the ages of 6 and 9 weeks.

aP=0.0072 vs. 6-week group, bP=0.0001 vs. 6-week group, cP<0.0001 vs. 6-week group, dP=0.0212 vs. 9-week group, eP<0.0001 vs. 9-week group, fP<0.0001 vs. 12-week group, gP<0.0001 vs. 15-week group

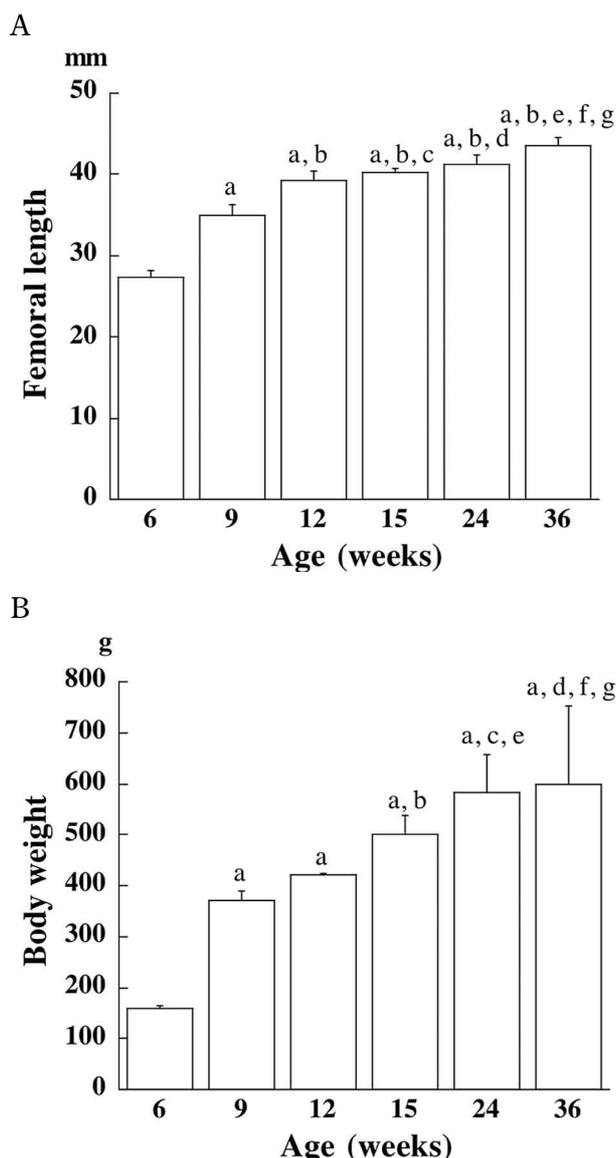


Figure 5A, B. Femoral length and body weight. Femoral length (A). The femoral length of rats and body weight increased during development. The increase rate of the femoral length was greatest between the ages of 6 and 9 weeks. aP< 0.0001 vs. 6-week group, bP< 0.0001 vs. 9-week group, cP= 0.0307 vs. 12-week group, dP=0.0001 vs. 12-week group, eP< 0.0001 vs. 12-week group, fP=0.0002 vs. 15-week group, gP= 0.0424 vs. 24-week group. Body weight (B). The body weight of rats increased during development. The increase rate of body weight was greatest between the ages of 6 and 9 weeks. The increase rate of body weight was the greatest between the ages of 6 and 9 weeks (B). aP< 0.0001 vs. 6-week group, bP=0.0090 vs. 9-week group, cP= 0.0001 vs. 9-week group, dP< 0.0001 vs. 9-week group, eP= 0.0017 vs. 12-week group, fP=0.0007 vs. 12-week group, gP= 0.0429 vs. 15-week group.

Correlations of M/M ratio with other biomechanical parameters.

There are significant positive correlations between M/M ratio and other parameters including total

BMD ($r=0.8127$, $p<0.0001$), periosteal circumference ($r=0.7441$, $p<0.0001$), endosteal circumference ($r=0.6667$, $p=0.0002$), ultimate load to failure ($r=0.7957$, $p<0.0001$), and stiffness of rat femur ($r=0.8150$, $p<0.0001$).

DISCUSSION

The M/M ratio by FTIR spectroscopy increases in proportion with development as total BMD, and bone strength increases. The M/M ratio indicates the relative amount of minerals and matrix contents and bone mineralization (6). The strength of the femoral shaft depends on the cortical bone, because the diaphyses of long bones are formed mostly by cortical tissue (14, 15). Increased mineralization of the diaphysis causes an increase in bone strength with development. In addition, there are significant positive correlations between M/M ratio and other parameters including total BMD, periosteal and endosteal circumferences, ultimate load to failure, and stiffness of rat femur. Based on these facts, the M/M ratio determines the biomaterial and biomechanical properties of bone.

Interestingly, the rates of increases of the M/M ratio, total BMD, and bone strength, femoral length of the rat femur, and body weight were greatest between 6 and 9 months of age, indicating that mineralization shown as the M/M ratio of the rat femur highly accelerated at this age. In addition, the M/M ratio of the rat femur by FTIR spectroscopy exceeded 1.0 between the ages of 6 and 9 weeks, showing that between these ages, the relative mineral content exceeded that of matrix content.

Both periosteal and endosteal circumferences of the femoral shaft of rats increased during development, indicating that both inner and outer diameters increased during development. The increase of periosteal circumference of the femoral shaft indicates acceleration of periosteal bone formation by osteoblasts compared with bone resorption by osteoclasts. In contrast, the increased endosteal circumference indicates acceleration of endosteal bone resorption by osteoclasts compared with bone formation by osteoblasts. The width of the cortical bone of the femoral shaft increases with development, indicating that periosteal bone formation overwhelms endosteal bone resorption of the rat femur.

In conclusion, the M/M ratio increases in proportion with development as bone quantity and bone

strength increase. Based on this finding, the M/M ratio is one of the determinants of the biomaterial and biomechanical properties of bone.

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