

1 **Overcoming thickened pathological skin in psoriasis via iontophoresis combined with**  
2 **tight junction-opening peptide AT1002 for intradermal delivery**  
3 **of NF- $\kappa$ B decoy oligodeoxynucleotide**

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19

1 **Abstract**

2 Transdermal delivery of nucleic acid therapeutics has been demonstrated to be effective for  
3 psoriasis treatment. We previously reported the utility of iontophoresis (IP) using weak electric  
4 current (0.3-0.5 mA/cm<sup>2</sup>) for intradermal delivery of nucleic acid therapeutics via weak  
5 electricity-mediated intercellular junction cleavage, and subsequent exertion of nucleic acid function.  
6 However, the thickened pathological skin in psoriasis hampers permeation of IP-administered  
7 macromolecules. Thus, approaches are needed to more strongly cleave intercellular spaces and  
8 overcome the psoriatic skin barrier. Herein, we applied a combination of tight junction-opening  
9 peptide AT1002 with IP, as synergistic effects of weak electricity-mediated intercellular junction  
10 cleavage and the tight junction-opening ability of AT1002 may help overcome thickened psoriatic  
11 skin and facilitate macromolecule delivery. Pretreatment with IP of an AT1002 analog exhibiting  
12 positively-charged moieties before fluorescence-labeled oligodeoxynucleotide IP resulted in the  
13 oligodeoxynucleotide permeation into psoriatic skin, whereas IP of the oligodeoxynucleotide alone  
14 did not. Moreover, psoriasis-induced upregulation of inflammatory cytokine mRNA levels was  
15 significantly suppressed by NF-κB decoy oligodeoxynucleotide IP combined with the AT1002 analog,  
16 resulting in amelioration of epidermis hyperplasia. These results suggest that synergistic effects of IP  
17 and an AT1002 analog can overcome thickened psoriatic skin and enable intradermal delivery of  
18 NF-κB decoy oligodeoxynucleotide for psoriasis treatment.

19

20 **Keywords**

21 Transdermal drug delivery; Iontophoresis; Nucleic acid therapeutics; NF-κB decoy  
22 oligodeoxynucleotide; AT1002; Psoriasis

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## 1 **1. Introduction**

2 Psoriasis is an immune-mediated disease that causes chronic skin inflammation and affects  
3 approximately 2–3% of the general population worldwide (Goldminz et al., 2013).  
4 Hyperproliferation and aberrant differentiation of keratinocytes is reported to be induced in psoriasis  
5 by dysregulated immune response, and proliferating keratinocytes secrete several cytokines to  
6 migrate immune cells including T cells and leukocytes into epidermis and dermis layers of inflamed  
7 psoriatic skin (Hawkes et al., 2017). These abnormal inflammatory reactions cause epidermis  
8 hyperplasia, the most distinctive histological changes in psoriasis that differ from other inflammatory  
9 skin diseases (Tonel and Conrad, 2009). Although the pathogenesis of psoriasis is not fully  
10 understood, systemic treatment with anti-tumor necrosis factor- $\alpha$  (TNF- $\alpha$ ) monoclonal antibody and  
11 anti-interleukin-17A (IL-17A) antibody has been clinically proven to inhibit immune responses and  
12 the pathological progression of psoriasis. Treatment of psoriasis with such antibody drugs is reported  
13 to be effective via modulation of the nuclear factor- $\kappa$ B (NF- $\kappa$ B) signaling pathway, a main regulator  
14 of immune responses (Veilleux and Shear, 2017). However, systemic administration of these drugs  
15 may be associated with adverse side effects, so that development of therapeutic approaches via  
16 topical routes, with minimal side effects, is required.

17 Transdermal delivery of nucleic acid therapeutics, such as small interfering RNA (siRNA)  
18 and nuclear factor- $\kappa$ B (NF- $\kappa$ B) decoy oligodeoxynucleotide (ODN), is a promising strategy for  
19 treatment of skin diseases, such as atopic dermatitis and psoriasis (Hashim et al., 2010; Mandal et al.,  
20 2020). Compared with invasive administration methods using needles, topical delivery is a  
21 non-invasive and patient-compliant method, and is therefore attracting considerable attention as a  
22 new administration route of nucleic acids with a favorable safety profile (Anselmo et al., 2019).  
23 While hydrophobic drugs with low molecular weights are generally suitable for transdermal delivery,  
24 delivery of nucleic acid therapeutics has typically been challenging owing to their high molecular  
25 weights and the presence of rigid skin barriers (Prausnitz and Langer, 2008). Recently, however,  
26 several technologies, including electroporation (Banga and Prausnitz, 1998), microneedles (Mikszta

1 et al., 2002), ionic liquid (Dharamdasani et al., 2020), and iontophoresis (IP) (Hashim et al., 2010),  
2 have been reported to enable successful delivery of nucleic acids into the skin. These approaches  
3 have also been applied for transdermal delivery of other macromolecular drugs, including proteins  
4 and nucleic acid therapeutics (Anselmo et al., 2019).

5         Among transdermal technologies described above, we demonstrated the utility of the IP  
6 using a weak electric current (0.3–0.5 mA/cm<sup>2</sup>). This system is non-invasive and does not require the  
7 use of needles (Hasan et al., 2020). IP has mostly been applied for transdermal delivery of  
8 hydrophobic and charged low-molecular weight drugs, such as lidocaine and dexamethasone, via  
9 electroosmosis and electropulsion (Guy et al., 2000; Lark and Gangarosa Sr, 1990; Spierings et al.,  
10 2008). However, we succeeded in the intradermal delivery of several hydrophilic macromolecules,  
11 such as nucleic acid therapeutics (siRNA and CpG oligo DNA) (Kigasawa et al., 2010; Kigasawa et  
12 al., 2011), antibodies (Fukuta et al., 2020), and charged nanoparticles (liposomes and nanogels)  
13 (Kajimoto et al., 2011; Toyoda et al., 2015), and demonstrated the subsequent exertion of their  
14 respective functions *in vivo*. In particular, we demonstrated efficient silencing of target mRNA by  
15 iontophoretic delivery of siRNA into the skin of atopic dermatitis model rats (Kigasawa et al., 2010).  
16 Results of another study from our laboratory provided insights into the mechanism of IP-mediated  
17 permeation of macromolecules into the skin. In particular, Ca<sup>2+</sup> influx into skin cells and subsequent  
18 intracellular signal activation are induced via IP, which leads to a decrease in expression of gap  
19 junction protein connexin 43 and depolymerization of tight junction-associated polymerized actin,  
20 resulting in cleavage of intercellular junctions (Hama et al., 2014). Moreover, treatment with weak  
21 electric current can induce cellular uptake of siRNA via a unique endocytosis process, in which  
22 endosomes are formed that can leak substances with molecular weights <70,000 that were taken up  
23 by cells; these findings explain how siRNA reaches the cytoplasm of IP-treated skin tissue (Hasan et  
24 al., 2016a; Hasan et al., 2016b; Torao et al., 2020). Based on these findings, if nucleic acid  
25 therapeutics (e.g., NF-κB decoy ODN and siRNA) can successfully be intradermally delivered into  
26 psoriatic skin via IP, it is expected that transdermal delivery of nucleic acid therapeutics by IP could

1 be applied for the treatment of not only atopic dermatitis but also other inflammatory skin diseases  
2 including psoriasis. However, we recently found that antibodies (Fukuta et al., 2020) and  
3 fluorescence-labeled ODN (data are shown in Results section) delivered by IP were unable to  
4 permeate the thickened pathological skin associated with psoriasis conditions. As a result of this  
5 finding, in our previous reports on psoriasis treatment by IP of an anti-tumor necrosis factor (TNF)- $\alpha$   
6 antibody, multiple doses were needed to obtain therapeutic effects, whereas a single dose hardly  
7 ameliorated psoriasis. These results were suggested to be due to formation of a thickened skin barrier  
8 caused by epidermis hyperplasia, a distinct symptom of psoriasis, which is caused by excessively  
9 aberrant keratinocyte differentiation and immune cell migration in psoriatic skin (Lowe et al., 2007).  
10 Hence, to overcome the thickened pathological skin barrier and achieve efficient treatment of  
11 psoriasis, approaches are needed, in addition to IP, to more strongly cleave the intercellular spaces.

12 To achieve efficient delivery of macromolecular drugs into psoriatic skin through  
13 transdermal route, we focused on the functional peptide AT1002, which was reported to exhibit tight  
14 junction-opening abilities (Goldblum et al., 2011). AT1002 is a synthetic six-mer peptide  
15 (Phe-Cys-Ile-Gly-Arg-Leu) identified from structure-activity relationship studies of Zonula occludens  
16 toxin (Zot), which can reversibly open tight junctions (Watts et al., 2005). AT1002 retains the tight  
17 junction-opening ability of Zot without the associated toxicity, and can decrease the expression of  
18 tight junction proteins resulting in promotion of paracellular transport of combined administered  
19 drugs across the epithelial barrier in nasal mucosa and intestine (Song et al., 2008a, b). Uchida et al.  
20 reported that topical application of AT1002 to tape-stripped mouse dorsal skin that lacks a skin barrier  
21 stratum corneum (SC) reversibly reduced ZO-1 expression, which led to increased intradermal  
22 delivery efficiency of siRNA into the healthy skin without SC (Uchida et al., 2011b). Uchida et al.  
23 also demonstrated that topically applied siRNA combined with AT1002 and a cell penetrating peptide  
24 to promote cellular uptake of siRNA could suppress target mRNA expression and ameliorate  
25 apoptotic symptoms (increase in ear thickness) in the ear skin of atopic dermatitis model mice  
26 (Uchida et al., 2011a). These findings highlight the usefulness of the tight junction-opening peptide

1 AT1002 for intradermal delivery of siRNA. However, it was reported that under psoriatic conditions,  
2 anomalous tight junctions are present in thickened pathological epidermis by broad localization of  
3 tight junction proteins, including ZO-1 from the stratum spinosum to the stratum granulosum  
4 (Kirschner et al., 2009). Therefore, if AT1002 can be transdermally delivered into broader and deeper  
5 regions of the inflamed thickened skin (i.e., relative to topical application), AT1002 is expected to  
6 regulate the anomalous tight junctions in psoriatic skin via reduction of ZO-1 expression, thus  
7 overcoming the thickened psoriatic skin barrier for transdermal delivery of nucleic acid therapeutics.

8         Considering the above findings, we hypothesized that combination of IP and AT1002 may  
9 overcome the abnormal skin barrier under psoriatic conditions. Combination of IP and AT1002 may  
10 result in AT1002 being intradermally delivered into deep regions of psoriatic skin to allow for  
11 synergistic effects of the tight junction-opening ability of AT1002 and intercellular junction cleavage  
12 via weak electricity to promote intradermal permeation of IP-administered nucleic acid therapeutics.  
13 However, the intradermally delivered nucleic acid therapeutics (e.g. NF- $\kappa$ B decoy ODN and siRNA)  
14 must be taken up by skin cells and reach the cytoplasm to exert their functions. Thus, another  
15 advantage of the combination of IP and AT1002 is that since IP induces cellular uptake of  
16 macromolecular drugs via unique endocytosis, and resultant endosomes can leak macromolecules  
17 with molecular weight <70,000, the intradermally permeated nucleic acid therapeutics may be  
18 efficiently taken up by inflamed skin cells. To prove this hypothesis, we herein used NF- $\kappa$ B decoy  
19 ODN as a representative nucleic acid therapeutic and applied the combination system of IP and  
20 AT1002 in psoriasis model rats. NF- $\kappa$ B is a key regulatory element in various inflammatory  
21 pathways, and is known to be a crucial mediator involved in pathological progression of psoriasis,  
22 which causes chronic inflammatory symptoms in the skin (Goldminz et al., 2013). Psoriatic  
23 inflammation is induced by marked activation of NF- $\kappa$ B pathways, followed by excess production of  
24 inflammatory cytokines, such as TNF- $\alpha$ , IL-1, IL-6, IL-17, etc. Hence, selective inhibition of NF- $\kappa$ B  
25 signaling by intradermal delivery of NF- $\kappa$ B decoy ODN is considered a promising approach to treat  
26 psoriasis (Gilmore and Garbati, 2010; Isomura and Morita, 2006).

1            In the present study, we first examined intradermal delivery of fluorescence-labeled NF- $\kappa$ B  
2    decoy ODN via IP alone and evaluated the effect of combination with AT1002 on its distribution in  
3    the inflamed skin of psoriasis model rats. We investigated the function of NF- $\kappa$ B decoy ODN  
4    delivered via combination of IP and AT1002 in the model rats, and also evaluated the therapeutic  
5    effects on psoriasis.

6

## 1 **2. Material and Methods**

2

### 3 **2.1. Reagents**

4 NF- $\kappa$ B decoy oligodeoxynucleotide (ODN) and 6-carboxyfluorescein (FAM)-labeled NF- $\kappa$ B  
5 decoy ODN (FAM-ODN; FAM labeling at the 3' end) were synthesized by Eurofins Genomics  
6 (Tokyo, Japan). The sequences of the NF- $\kappa$ B decoy ODN were as follows:  
7 5'-CCTTGAAGGGATTTCCCTCC-3' and 5'-GGAACTTCCCTAAAGGGAGG-3'. The AT1002  
8 analog (Arg-Arg-Arg-Gly-Gly-Phe-Cys-Ile-Gly-Arg-Leu) and the control 10-mer peptide having  
9 three Arg and two Gly without the sequences of AT1002  
10 (Arg-Arg-Arg-Gly-Gly-Leu-Gly-Cys-Arg-Phe-Ile) were synthesized by Peptide Institute, Inc. (Osaka,  
11 Japan). Fluorescein isothiocyanate (FITC)-labeled AT1002 analog (FITC- $\epsilon$ -aminocaproic  
12 acid-Arg-Arg-Arg-Gly-Gly-Phe-Cys-Ile-Gly-Arg-Leu) was also synthesized by Peptide Institute, Inc.  
13 Beselna cream 5%<sup>®</sup> was purchased from Mochida Pharmaceuticals (Tokyo, Japan). OCT compound,  
14 Perma Fluor Aqueous Mounting Medium, and Entellan New<sup>®</sup> (hydrophobic mounting medium) were  
15 obtained from Sakura Finetek (Tokyo, Japan), Thermo Fisher Scientific (Tokyo, Japan), and Merck  
16 Millipore (Tokyo, Japan), respectively. Isoflurane, Mayer's hematoxylin solution and 1% eosin Y  
17 solution were purchased from FujiFilm Wako Pure Chemical (Osaka, Japan). QIAzol Lysis reagent  
18 and RNeasy Plus Universal Midi Kit were obtained from QIAGEN (Hilden, Germany). PrimeScript  
19 RT Master Mix (Perfect Real Time) and TB Green<sup>™</sup> Premix Ex Taq<sup>™</sup> II (Tli RNaseH Plus) were  
20 purchased from Takara Bio (Shiga, Japan). All other reagents used in this study were of the highest  
21 grade available commercially.

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### 23 **2.2. Animals**

24 Seven-week-old male Wistar rats (190-210 g) were purchased from Japan SLC, Inc.  
25 (Shizuoka, Japan). All animal experiments were evaluated and approved by the Animal and Ethics  
26 Review Committee of Tokushima University.

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### **2.3. Preparation of psoriasis model rats**

Psoriasis model rats were prepared as previously reported (Fukuta et al., 2020; Satake et al., 2018). Briefly, rats were anesthetized and maintained with 3% and 1.5% isoflurane, respectively. The dorsal skins of the rats were shaved, and 60 mg of imiquimod (IMQ) cream (Beselna cream 5%; 3 mg equivalent as IMQ) was topically applied onto a 6-cm<sup>2</sup> region of the dorsal skin, after which the rats were allowed to recover from anesthesia. IMQ treatment was conducted four times per 24 h to induce psoriasis, and the psoriasis model rats were used in the following experiments. To confirm induction of psoriasis, the skin of the rats was removed 24 h after the 4<sup>th</sup> IMQ treatment and embedded in OCT compound, followed by freezing with dry ice/ethanol. Frozen skin sections were cut into 10- $\mu$ m thick sections using a cryostat (CM3050S; Leica Biosystems, Tokyo, Japan). Thereafter, hematoxylin-eosin (HE) staining was performed to observe epidermis hyperplasia, a distinct symptom of psoriasis, as described below (2.4. HE staining of rat skin).

### **2.4. HE staining of rat skin**

The prepared 10- $\mu$ m frozen skin sections as described above (2.3. Preparation of psoriasis model rats) were fixed with 4% PFA for 10 min in humidified chamber. After washing with phosphate-buffered saline (PBS), the sections were stained with Mayer's hematoxylin solution for 10 min at room temperature, washed with distilled water, and subsequently stained with 1% eosin Y solution for 1 min at room temperature. The sections were then dehydrated with 80–100% ethanol, cleared with xylene, and mounted with hydrophobic mounting medium (Entellan New<sup>®</sup>). Thereafter, the sections were observed with a fluorescence phase contrast microscope (BZ-9000, Keyence, Osaka, Japan).

### **2.5. Iontophoresis (IP)**

IP of NF- $\kappa$ B decoy-ODN and the AT1002 analog was performed in accordance with our

1 previous report with slight modifications (Fukuta et al., 2020; Hama et al., 2014). Briefly, Wistar rats  
2 were anesthetized by intraperitoneal injection of chloral hydrate (400 mg/kg rat) dissolved in PBS,  
3 and the dorsal skin of the rats was shaved with a hair shaver. PBS used in the present study was  
4 composed of 137 mM NaCl, 2.7 mM KCl, 10 mM Na<sub>2</sub>HPO<sub>4</sub>·12H<sub>2</sub>O, and 1.8 mM KH<sub>2</sub>PO<sub>4</sub>. For  
5 administration of FAM-ODN, nonwoven fabric (1 cm<sup>2</sup>) containing 10 µg (in 100 µL RNase free  
6 water) of ODN solution was placed on the dorsal skin, and a nonwoven fabric (1 cm<sup>2</sup>) moistened  
7 with 100 µL of PBS was also placed 1 cm away. Each nonwoven fabric containing ODN or PBS was  
8 attached to a Ag-AgCl electrode (3M Health Care, Minneapolis, MN, USA) with a surface area of 1  
9 cm<sup>2</sup>. The Ag-AgCl electrodes with nonwoven fabric containing ODN or PBS were connected to the  
10 cathode and anode of a power supply (TTI ellebeau Inc., model TCCR-3005, Tokyo, Japan),  
11 respectively. The connections were covered with tape, and IP was then performed with a constant  
12 current of 0.34 mA/cm<sup>2</sup> (0.34 mA) for 1 h.

13 For pretreatment of the skin with the AT1002 analog, nonwoven fabric (1 cm<sup>2</sup>) containing  
14 1058 µg of the AT1002 analog (in 100 µL deionized distilled water; 400 µg equivalent as AT1002)  
15 was attached to the Ag-AgCl electrode, and the electrode was connected to the anode of the power  
16 supply (Cathode: PBS), followed by 1 h of IP (0.34 mA). Pretreatment by IP administration of the  
17 AT1002 analog was performed 2 h prior to the start of IP administration of ODN, and the electrode  
18 with nonwoven fabric containing ODN was attached to the same position as that containing the  
19 AT1002 analog. Thereafter, IP was performed (0.34 mA for 1 h). To evaluate the effect of the  
20 IP-administered control 10-mer peptide, nonwoven fabric containing 400 µg of the peptide (in 100  
21 µL deionized distilled water) was attached to the Ag-AgCl electrode, and anodal IP (0.34 mA for 1 h)  
22 was performed.

23

## 24 **2.6. Intradermal distribution of fluorescence-labeled oligodeoxynucleotide**

25 IP of FAM-ODN was performed in accordance with above-mentioned procedures (2.5.  
26 Iontophoresis (IP)). Immediately after 1-h IP of FAM-ODN, 10-µm frozen skin sections were

1 prepared as described above (2.3. Preparation of psoriasis model rats). The 10- $\mu$ m thick frozen skin  
2 sections were attached to MAS-coated slide glasses and mounted with Perma Fluor Aqueous  
3 Mounting Medium. FAM fluorescence in the skin sections was observed using a confocal laser  
4 scanning microscope (LSM700, Carl Zeiss, Jena, Germany). Average delivery depth of FAM-ODN  
5 from the skin surface was determined using image analysis software (NIH ImageJ), and was  
6 calculated from over 5 images per rat in each group in accordance with our previous report with  
7 slight modifications (Kajimoto et al., 2011).

8

### 9 **2.7. Intradermal distribution of IP-administered FAM-labeled ODN in psoriatic skin**

10 At 24 h after the 4<sup>th</sup> IMQ treatment on the dorsal skin of rats, pretreatment with  
11 IP-administered AT1002 analog (400  $\mu$ g AT1002 dose in 100  $\mu$ L) or with control 10-mer peptide  
12 (400  $\mu$ g peptide dose in 100  $\mu$ L), and IP administration of FAM-ODN (50  $\mu$ g in 100  $\mu$ L) was  
13 performed as described above (2.5. Iontophoresis (IP)). At 0 h after 1-h IP for FAM-ODN, the  
14 psoriatic skin was collected and frozen with dry ice/ethanol, and 10- $\mu$ m frozen skin sections were  
15 prepared with a cryostat. After mounting the sections with Perma Fluor Aqueous Mounting Medium,  
16 FAM fluorescence in the skin was observed by confocal laser scanning microscopy. Average delivery  
17 depth of FAM-ODN from the psoriatic skin surface was calculated using the ImageJ software, and  
18 was calculated from over 5 images per rat in each group.

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### 20 **2.8. Intradermal distribution of fluorescence-labeled AT1002 analog in healthy and psoriatic** 21 **skin**

22 To evaluate intradermal distribution of FITC-labeled AT1002 analog, nonwoven fabric (1  
23 cm<sup>2</sup>) containing 16 (for healthy rats) or 80  $\mu$ g (for psoriasis model rats) of the peptide (dissolved in  
24 100  $\mu$ L deionized distilled water) was attached to the Ag-AgCl electrode, followed by connecting to  
25 the anode of the power supply. After 0 or 2 h after 1-h IP, frozen skin sections of healthy and  
26 IMQ-treated psoriatic model rats were prepared as described above (2.6. Intradermal distribution of

1 fluorescence-labeled oligodeoxynucleotide), and FITC fluorescence in the skin sections was  
2 observed with a confocal laser scanning microscope.

3

#### 4 **2.9. IP of NF- $\kappa$ B decoy ODN in the psoriasis model**

5 At 24 h after the 4<sup>th</sup> IMQ treatment, IMQ-induced psoriasis model rats were anesthetized  
6 with chloral hydrate (400 mg/kg rat). Nonwoven fabric (1 cm<sup>2</sup>) containing 50  $\mu$ g NF- $\kappa$ B decoy ODN  
7 solution (in 100  $\mu$ L of RNase free water) was attached to a Ag-AgCl electrode with a surface area of  
8 1 cm<sup>2</sup>, and applied onto the psoriatic skin. Electrodes with nonwoven fabric containing NF- $\kappa$ B decoy  
9 ODN or PBS were connected to the cathode and anode of the power supply, respectively. IP was  
10 performed with a constant current of 0.34 mA/cm<sup>2</sup> (0.34 mA) for 1 h. For pretreatment of the  
11 psoriatic skin with the AT1002 analog, IP administration of the AT1002 analog (1058  $\mu$ g in 100  $\mu$ L  
12 deionized distilled water; 400  $\mu$ g equivalent as AT1002) was performed as described above (2.5.  
13 Iontophoresis (IP)). At 24 h after IP treatment, the rats were euthanized, and the skin tissue of the rats  
14 under the cathode was removed and used in the following experiments.

15

#### 16 **2.10. RNA extraction**

17 After removal of the skin tissue of the rats, RNA extraction was performed as described  
18 previously with slight modifications (Howe et al., 2018; Robbe-Saule et al., 2017). Briefly, 0.5 cm<sup>2</sup>  
19 of cut skin was homogenized in 4 mL of QIAzol Lysis reagent using a TissueRuptor II (QIAGEN).  
20 After 5 min incubation at room temperature, total RNA was purified and extracted with an RNeasy  
21 Plus Universal Midi Kit according to the manufacturer's instructions. The total RNA concentration  
22 was quantified using a Nanodrop 8000 (Thermo Fisher Scientific).

23

#### 24 **2.11. Quantitative analysis of mRNA expression by real-time reverse transcription polymerase** 25 **chain reaction (RT-PCR)**

26 By using extracted RNA, real-time RT-PCR was performed as described previously with

1 slight modifications (Shimokawa et al., 2020). Briefly, cDNA was synthesized from 200 ng of total  
2 RNA with PrimeScript RT Master Mix (Perfect Real Time) using a MJ Mini Personal Thermal  
3 Cycler (Bio-Rad, Hercules, CA, USA). The conditions for the reverse transcription reaction were  
4 37°C for 15 min, whereas that for inactivation of reverse transcriptase were 85°C for 5 sec. Real-time  
5 RT-PCR analysis was performed with TB Green™ Premix Ex Taq™ II (Tli RNaseH Plus) using a  
6 Thermal Cycler Dice Real Time System III (Takara Bio). For analysis of the mRNA expression  
7 levels of TNF- $\alpha$ , IL-6, and GAPDH, the cDNA was denatured at 95°C for 30 sec, followed by 40  
8 cycles of 95°C for 5 sec and 60°C for 30 sec for amplification. The primers were synthesized by  
9 Eurofins Genomics, and those sequences used for the real-time RT-PCR are shown in Table 1.  
10 mRNA levels of TNF- $\alpha$  and IL-6 were calculated using the  $2^{-\Delta\Delta Ct}$  method by normalization relative to  
11 GAPDH mRNA levels. The relative transcript levels (TNF- $\alpha$ /GAPDH mRNA and IL-6/GAPDH  
12 mRNA) were calculated to compare the differences between each group.

13

## 14 **2.12. Evaluation of epidermis layer thickness**

15 Pretreatment of IP-administered AT1002 analog and IP administration of NF- $\kappa$ B decoy  
16 ODN were performed as mentioned above (2.9. IP of NF- $\kappa$ B decoy ODN in the psoriasis model) in  
17 IMQ-treated psoriasis model rats, followed by preparation of frozen skin sections 24 h IP  
18 administration of NF- $\kappa$ B decoy ODN. The 10- $\mu$ m frozen skin tissues of each group of psoriasis  
19 model rats were stained with HE and observed using a fluorescence phase contrast microscope  
20 (BZ-9000). Average epidermis layer thickness was determined from >20 images per rat with the  
21 image analysis software of BZ-9000.

22

## 23 **2.13. Statistical analysis**

24 Statistical differences were evaluated by one-way analysis of variance with the Tukey  
25 post-hoc test. Data are presented as mean  $\pm$  standard deviation (S.D.).

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### 1 **3. Results**

2

#### 3 **3.1. Intradermal distribution of fluorescence-labeled oligodeoxynucleotides administered via IP** 4 **in healthy and psoriatic skin**

5 We performed transdermal delivery of FAM-ODN by IP on the dorsal skin of healthy and  
6 IMQ-treated psoriasis model rats. Images of HE staining obtained from both rats showed that  
7 epidermis hyperplasia, a symptom of psoriasis, was observed in IMQ-treated rats but not in untreated  
8 healthy rats (Figs 1A and B), indicating that psoriatic inflammation was induced by repeated topical  
9 application of IMQ cream, consistent with previous reports (Satake et al., 2018). For topical skin  
10 application of FAM-ODN, FAM fluorescence was only observed on the stratum corneum, as judged  
11 from HE staining, and hardly detected in skin tissues (Fig. 1C). No fluorescence was observed in the  
12 group receiving iontophoretic treatment alone (Fig. 1D). When FAM-ODN was administered via IP,  
13 fluorescence of FAM-ODN was clearly observed from the epidermis to the dermis layer of healthy  
14 skin at immediately after 1-h IP (Fig. 1E), consistent with our previous reports on intradermal  
15 delivery of nucleic acid therapeutics (e.g., siRNA and CpG-DNA) via IP (Kigasawa et al., 2010;  
16 Kigasawa et al., 2011). However, in IMQ-treated psoriasis model rats, IP-mediated intradermal  
17 permeation of FAM-ODN was hardly observed and fluorescence was detected only on the surface of  
18 the epidermis layer (Fig. 1F), suggesting that psoriatic skin barriers (due to epidermis hyperplasia)  
19 hampered permeation of ODN via IP. On the other hand, no obvious skin damage was observed by IP  
20 treatment both in healthy and IMQ-treated psoriasis model rats as shown in pictures of dorsal skin of  
21 the rats and the images of HE staining (Supplementary Fig. 1).

22

#### 23 **3.2. Intradermal delivery of NF- $\kappa$ B decoy ODN into thickened psoriatic skin via IP combined** 24 **with the AT1002 analog**

25 As transdermal permeation of FAM-ODN could not be achieved by IP alone, we sought to  
26 overcome the thickened psoriatic skin barrier by a combination of IP and the tight junction-opening

1 peptide AT1002 (Phe-Cys-Ile-Gly-Arg-Leu). As the electric charge of AT1002 is nearly neutral (or  
2 weakly positive), the delivery efficiency of AT1002 via IP was considered to be low. Hence, to make  
3 the physicochemical property of AT1002 more suitable for IP, we designed an AT1002 analog  
4 (Arg-Arg-Arg-Gly-Gly-Phe-Cys-Ile-Gly-Arg-Leu), in which the AT1002 peptide was ligated with  
5 two Gly spacers and three Arg residues (positively charged moieties). At first, we prepared a  
6 complex of FAM-ODN and the AT1002 analog via electrostatic interaction and subsequently  
7 performed IP of the complex. However, intradermal permeation of the complex could not be  
8 observed, even in healthy skin (data not shown). We then examined the effect of pretreatment by IP  
9 administration of the AT1002 analog on the intradermal delivery efficiency of FAM-ODN. To  
10 determine the appropriate timing of IP treatment with the AT1002 analog prior to FAM-ODN IP, we  
11 performed IP of the AT1002 analog at different time points, namely 1, 3, or 6 h prior to FAM-ODN  
12 IP, using healthy rats. For these experiments, electrodes with nonwoven fabric containing the AT1002  
13 analog and FAM-ODN were set at the same skin positions. Results of these preliminary experiments  
14 showed that, although transdermal permeation of FAM-ODN tended to increase by the pretreatment  
15 with AT1002 analog IP performed 1 or 6 h before the start of FAM-ODN IP, significant increase in  
16 permeation of FAM-ODN was observed following pretreatment with the AT1002 analog at 3 h prior  
17 to the start of FAM-ODN IP (Supplementary Fig. 2). Thus, we decided to carry out pretreatment with  
18 the AT1002 analog IP at 3 h prior to the start of IP of FAM-ODN, as shown in Fig. 2A. Confocal  
19 microscopic images of healthy skin treated with a combination of IP with the AT1002 analog and  
20 FAM-ODN showed that FAM fluorescence was more broadly and brightly observed compared with  
21 IP alone (Figs. 2B and D). Moreover, the depth of FAM-ODN delivery was significantly increased  
22 (2.9-fold) by a combination of IP with the AT1002 analog (Fig. 2E). On the other hand, in the group  
23 of pretreatment with the control 10-mer peptide (Arg-Arg-Arg-Gly-Gly-Leu-Gly-Cys-Arg-Phe-Ile),  
24 FAM fluorescence in the skin of healthy rats was almost similar to the group of FAM ODN IP alone  
25 (Fig. 2C). The quantitative analysis of penetration depth also showed that the pretreatment with IP of  
26 the control 10-mer peptide hardly affected the permeation of FAM-ODN (Fig. 2E), indicating that

1 enhancement of intradermal delivery of FAM-ODN was derived from the pretreatment with IP of the  
2 tight junction opening peptide AT1002.

3           Based on the results using healthy rats, we next investigated the combination IP system in  
4 IMQ-treated psoriasis model rats according to the experimental schedule shown in Fig. 2F. Similar to  
5 the results shown in Fig. 1F, efficient transdermal permeation of FAM-ODN was not observed in the  
6 group treated with IP alone (Fig. 2G). Also, the combination of FAM-ODN IP and pretreatment with  
7 the control peptide IP could not achieve efficient delivery of FAM-ODN into the psoriatic thickened  
8 skin (Fig. 2H). However, in the case of the combination of FAM-ODN IP and pretreatment with  
9 AT1002 analog IP, FAM fluorescence was broadly observed in the psoriatic skin, and also reached  
10 the dermis layer (Fig. 2I). Quantitative data on the depth of delivery of the ODN also indicated  
11 significant (7.8-fold) enhancement of intradermal permeation of FAM-ODN by a combination of IP  
12 and AT1002 analog pretreatment (Fig. 2J).

13

### 14 **3.3. Intradermal distribution of IP-administered fluorescence-labeled AT1002 analog in healthy** 15 **and psoriasis model rats**

16           By using FITC-labeled AT1002 analog, intradermal distribution of IP-administered AT1002  
17 analog in healthy and psoriasis model rats was investigated. In healthy rats, the FITC fluorescence  
18 was observed from the epidermis to the dermis layer of healthy skin at immediately after 1-h IP (Fig.  
19 3A). The fluorescence of the peptide remained in the epidermis and dermis layers 2 h after 1-h IP,  
20 namely at the timing of FAM-ODN IP (Fig. 3B). On the other hand, the FITC fluorescence was  
21 mainly observed in the thickened epidermis layer of the IMQ-treated psoriasis model rats at 0 h after  
22 1-h IP (Fig. 3C). Importantly, the FITC-labeled AT1002 analog reached the dermis layer of the  
23 psoriatic skin 2 h after IP administration of the peptide (Fig. 3D).

24

### 25 **3.4. Suppression of upregulation of inflammatory cytokine mRNA by combined IP treatment** 26 **with NF- $\kappa$ B decoy ODN and the AT1002 analog**

1 We investigated the biological function of NF- $\kappa$ B decoy ODN delivered into psoriatic skin  
2 via a combination of IP and AT1002 analog pretreatment. As NF- $\kappa$ B decoy ODN can inhibit  
3 transcriptional induction of various inflammatory cytokines (e.g., TNF- $\alpha$ , IL-6) via the  
4 transcriptional factor NF- $\kappa$ B, we evaluated the effect of IP-administered NF- $\kappa$ B decoy ODN on  
5 mRNA levels of TNF- $\alpha$  and IL-6. IP administration of NF- $\kappa$ B decoy ODN was performed on the  
6 psoriatic skin at 24 h after the 4<sup>th</sup> IMQ treatment, and mRNA levels of TNF- $\alpha$  and IL-6 were assessed  
7 at 24 h after IP, as shown in Fig. 4A. Results showed that IMQ treatment significantly increased  
8 mRNA levels of TNF- $\alpha$  and IL-6 in the skin of the psoriasis model rats (Figs. 4B and C). IP of  
9 NF- $\kappa$ B decoy ODN had almost no effect on TNF- $\alpha$  mRNA levels compared with IMQ-treated rats  
10 (Fig. 4B), while IL-6 mRNA levels tended to decrease (Fig. 4C). On the other hand, in the group  
11 receiving a combination of NF- $\kappa$ B decoy IP and pretreatment with AT1002 analog IP, TNF- $\alpha$  mRNA  
12 levels were significantly decreased (Fig. 4B). Moreover, the combination exhibited superior  
13 suppressive effects on IL-6 mRNA levels compared with the group receiving NF- $\kappa$ B decoy ODN IP  
14 alone (Fig. 4C).

15

### 16 **3.5. Therapeutic effect of combined IP delivery of NF- $\kappa$ B decoy ODN and the AT1002 analog** 17 **on psoriasis**

18 Finally, we investigated the therapeutic effect of combined IP delivery of NF- $\kappa$ B decoy  
19 ODN and the AT1002 analog in IMQ-induced psoriasis model rats by evaluating epidermis thickness  
20 as an indicator of epidermis hyperplasia after psoriatic inflammation. Images of HE staining showed  
21 that four IMQ treatments significantly increased epidermis thickness compared to untreated normal  
22 rats (Figs. 5A, B, and E). IP administration of NF- $\kappa$ B decoy ODN had almost no effect on epidermis  
23 hyperplasia compared with IMQ-treated rats (Figs. 5C and E). On the other hand, IP of NF- $\kappa$ B decoy  
24 ODN combined with pretreatment with IP-administered AT1002 analog significantly ameliorated  
25 epidermis hyperplasia compared with IMQ-treated rats and rats receiving NF- $\kappa$ B decoy ODN IP  
26 alone (Figs. 5D and E).

#### 1 **4. Discussion**

2 Our previous studies demonstrated the utility of IP using weak electric current (0.3–0.5  
3 mA/cm<sup>2</sup>) to enable intradermal delivery of hydrophilic macromolecules, such as nucleic acid  
4 therapeutics, antibodies, and nanoparticles (Fukuta et al., 2020; Kajimoto et al., 2011; Kigasawa et  
5 al., 2010). Based on the results of mechanistic studies, we found that IP-induced Ca<sup>2+</sup> influx and  
6 protein kinase C- $\alpha$  activation is related to the cleavage of intercellular junctions via gap junction  
7 dissociation by connexin 43 reduction and depolymerization of filamentous actin (Hama et al., 2014).  
8 However, under psoriasis conditions, the thickened pathological skin barrier exhibiting broad  
9 localization of tight junction proteins hampered intradermal permeation of IP-administered  
10 macromolecule drugs in our previous study (Fukuta et al., 2020). Moreover, in the present study,  
11 IP-administered FAM-ODN was unable to penetrate the thickened psoriatic skin, but was found to  
12 efficiently permeate the skin of healthy rats (Fig. 1). Hence, to achieve efficient delivery of  
13 macromolecules (including nucleic acid therapeutics), combination of IP with treatments capable of  
14 regulating intercellular junctions is required to overcome the psoriatic skin barrier.

15 To this end, we focused on the functional peptide AT1002 (Phe-Cys-Ile-Gly-Arg-Leu) to  
16 regulate tight junction in the skin. AT1002 was reported to exhibit tight junction-opening abilities  
17 (Goldblum et al., 2011; Uchida et al., 2011b). Combination of AT1002 with IP was expected to allow  
18 for synergistic effects of tight junction-opening activity associated with AT1002 and the intercellular  
19 cleavable effect of IP. Also, as weak electric current employed for IP can evoke endocytosis with  
20 unique properties that allow for easy leakage of substances with molecular weights <70,000 (Hasan  
21 et al., 2016b; Torao et al., 2020), intradermally delivered nucleic acid therapeutics may be efficiently  
22 taken up by the inflamed skin cells, and subsequently reach the cytoplasm to exert the functions.

23 We evaluated the combination effect of IP and pretreatment with IP of the AT1002 analog  
24 (Arg-Arg-Arg-Gly-Gly-Phe-Cys-Ile-Gly-Arg-Leu) on the intradermal delivery efficiency of  
25 FAM-ODN. The AT1002 analog containing positively charged moieties was designed to facilitate IP  
26 application of the peptide to deeply penetrate the skin. As shown in Figure 1, IP alone could deliver

1 FAM-ODN into the skin of healthy rats, whereas the combination of pretreatment with the AT1002  
2 analog IP was found to significantly enhance (2.9-fold) intradermal permeation of FAM-ODN (Figs.  
3 2A-E). In IMQ-treated psoriasis model rats, transdermal permeation of FAM-ODN was not observed  
4 upon treatment with IP alone (Fig. 2G). Surprisingly, the fluorescence of FAM extended from the  
5 thickened epidermis layer to the dermis layer by a combination of FAM-ODN IP and AT1002 analog  
6 pretreatment IP (Figs. 2I and J), indicating that the combination system could overcome the  
7 thickened psoriatic skin barrier and allow for intradermal permeation of nucleic acid therapeutics. On  
8 the other hand, the combination of FAM-ODN IP and pretreatment with IP of the control 10-mer  
9 peptide (Arg-Arg-Arg-Gly-Gly-Leu-Gly-Cys-Arg-Phe-Ile), which peptide was designed with three  
10 Arg and two Gly spacers without the sequences of the tight junction opening peptide AT1002, could  
11 not enhance transdermal permeation of FAM-ODN into both healthy and psoriatic thickened skins  
12 (Figs. 2C, E, H, J). These results indicate that enhancement of intradermal delivery of FAM-ODN  
13 was derived from the pretreatment with IP of AT1002 analog. It was previously reported that  
14 abnormal tight junctions associated with epidermal cell proliferation are formed in the psoriatic skin,  
15 and that expression of tight junction-related proteins, including occludin and ZO-1, extends to the  
16 stratum spinosum, which proteins are normally localized in the stratum granulosum (Kirschner et al.,  
17 2009). Also, keratinocytes in the epidermis of psoriatic skin were reported to be highly proliferative  
18 due to certain inflammatory cytokines, which leads to immune cell migration and epidermis  
19 hyperplasia (Lowe et al., 2007). Considering these findings and the results of the present study, it  
20 was suggested that a combination of weak electricity and the AT1002 analog could synergistically  
21 affect the state of the skin barrier composed of both abnormal tight junctions and proliferated cells  
22 via intercellular junction cleaving and tight junction-opening effects, respectively.

23 In the present study, we newly designed the AT1002 analog  
24 (Arg-Arg-Arg-Gly-Gly-Phe-Cys-Ile-Gly-Arg-Leu) to make the physicochemical property of AT1002  
25 more applicable for IP. Since application of IP for the original AT1002 (Phe-Cys-Ile-Gly-Arg-Leu)  
26 with insufficient charged residues is difficult and the effect of the original AT1002 cannot be

1 compared with the AT1002 analog, it is thought to be impossible to directly evaluate whether the  
2 activity of the AT1002 analog is the same as the original AT1002. However, in the present study, IP  
3 administration of the AT1002 analog promoted intradermal permeation of IP-administered  
4 FAM-ODN not only in healthy skin but also in psoriatic skin (Fig. 2). Therefore, it is considered that  
5 the designed AT1002 analog could have a similar tight junction-opening effect to the original  
6 AT1002.

7 From the experiments to decide the time schedule of pretreatment with AT1002 analog IP,  
8 although the pretreatment with the AT1002 analog IP at 1 or 6 h prior to the start of FAM-ODN IP  
9 tended to enhance FAM-ODN permeation into the skin, the pretreatment done 3 h prior to  
10 FAM-ODN IP significantly increased intradermal permeation of FAM-ODN (Supplementary Figure  
11 2). Based on these results, it was considered that certain time was needed for intradermally delivered  
12 AT1002 analog to exert its tight junction-opening activity to cause skin barrier function change,  
13 which change is enough to enable efficient intradermal permeation of the subsequently administered  
14 ODN. On the other hand, based on our previous reports regarding IP-mediated successful delivery of  
15 nucleic acid therapeutics (Kigasawa et al., 2010; Kigasawa et al., 2011) and considering the risk of  
16 skin burn and other adverse effects, we performed IP of the AT1002 analog and ODN for 1 h in this  
17 study.

18 Intradermal distribution of IP-administered AT1002 analog was also evaluated by using  
19 FITC-labeled AT1002 analog. The FITC fluorescence was extended from the epidermis to the dermis  
20 layer of healthy skin before the timing of IP administration of FAM-ODN (Figs. 3A and B). Although  
21 the FITC-labeled AT1002 analog was mainly distributed in the thickened epidermis layer  
22 immediately after 1- h IP, its fluorescence reached the dermis layer of the psoriatic skin at 2 h after  
23 1-h IP (Figs. 3C and D). These results suggest that the AT1002 analog administered via IP could  
24 exert its tight-junction opening activity and affect the state of the skin barrier of both healthy and  
25 psoriasis model rats. Consequently, it is suggested that the AT1002 analog pretreatment could

1 promote transdermal permeation of subsequently administered FAM-ODN, resulting in overcoming  
2 aberrant psoriatic thickened skin barrier.

3 Under psoriatic conditions, upregulation of several inflammatory cytokines, including  
4 TNF- $\alpha$  and IL-6, is induced by NF- $\kappa$ B activation. Indeed, mRNA levels of both TNF- $\alpha$  and IL-6  
5 were significantly increased in the dorsal skin of IMQ-treated psoriasis model rats (Fig. 4). IP  
6 administration of a single dose of NF- $\kappa$ B decoy ODN hardly affected mRNA levels of both cytokines.  
7 On the other hand, intradermal delivery of NF- $\kappa$ B decoy ODN by a combination of IP and AT1002  
8 analog pretreatment significantly reduced the levels of TNF- $\alpha$  mRNA and tended to decrease levels  
9 of IL-6 mRNA (Fig. 4B and C), suggesting that pretreatment with the AT1002 analog enabled  
10 efficient delivery of IP-delivered NF- $\kappa$ B decoy ODN and subsequent exertion of its function. For  
11 proper functioning of NF- $\kappa$ B decoy ODN, ODN needs to be taken up into the target cells and  
12 subsequently reach the cytoplasm. We previously reported that the weak electric current treatment  
13 used for IP can induce a unique endocytosis process to result in subsequent cytoplasmic delivery of  
14 nucleic acid therapeutics via activation of specific cellular signaling (Hasan et al., 2019). Therefore,  
15 it is suggested that IP may allow for not only intradermal delivery of NF- $\kappa$ B decoy ODN by  
16 combination with AT1002, but also for cytoplasmic delivery via weak electric current-induced  
17 unique endocytosis, resulting in suppression of upregulation of mRNA levels of inflammatory  
18 cytokines in psoriatic skin.

19 Finally, we evaluated therapeutic outcomes of IMQ-induced psoriasis model rats by  
20 treatment with NF- $\kappa$ B decoy ODN IP combined with pretreatment by AT1002 analog IP. IMQ  
21 treatment significantly induced epidermal hyperplasia, which was correlated with upregulation of  
22 levels of TNF- $\alpha$  and IL-6 mRNA (Figs. 5A, B, E). Although intradermal delivery of the ODN via IP  
23 alone hardly decreased the thickness of the epidermis, the ODN delivered by a combination of IP and  
24 AT1002 analog pretreatment significantly suppressed epidermal hyperplasia compared with the  
25 untreated group (Figs. 5C-E). It was previously reported that NF- $\kappa$ B signaling plays a crucial role in  
26 the progression of psoriasis pathology (Goldminz et al., 2013; Stratis et al., 2006; Xiao et al., 2017).

1 Under psoriasis conditions, activation of NF- $\kappa$ B signaling is induced in intradermal macrophages and  
2 keratinocytes, and leads to release of TNF- $\alpha$  and IL-6 from those cells, resulting in subsequent  
3 activation of Langerhans cells (a subset of dendritic cell) and T cells. Then, several inflammatory  
4 cytokines secreted from the activated cells further activate keratinocytes, and the pathology of  
5 psoriasis is exacerbated. In the present study, intradermal delivery of NF- $\kappa$ B decoy ODN via  
6 combination IP could suppress upregulation of mRNA levels of TNF- $\alpha$  and IL-6 in IMQ-treated  
7 psoriasis model rats. These results, combined with the findings from previous reports, suggest that  
8 inhibition of NF- $\kappa$ B signaling by the decoy ODN could suppress a series of immune reactions,  
9 resulting in amelioration of epidermal hyperplasia. Based on these results, it is suggested that  
10 intradermal delivery of NF- $\kappa$ B decoy ODN via IP combined with AT1002 analog pretreatment could  
11 be useful for the treatment of psoriasis.

12 To exert the functionality of the NF- $\kappa$ B decoy ODN, its stability in the skin and influence of  
13 the IP treatment on the stability are needed to be considered. In the present study, NF- $\kappa$ B decoy ODN  
14 intradermally delivered by combination with AT1002 analog IP pretreatment showed significant  
15 therapeutic effect in IMQ-treated psoriasis model rats. Also, in our previous studies, we succeeded in  
16 intradermal delivery of other nucleic acid therapeutics siRNA and CpG-ODN into the skin and  
17 exertion of their respective effects, namely target mRNA knockdown effect and induction of immune  
18 responses against cancer (Kigasawa et al., 2010; Kigasawa et al., 2011). These results suggest that  
19 the intradermally delivered ODN could be stable in the psoriatic skin and exert its function. Although  
20 the period of the ODN been stable in the skin is unclear, weak electric current was previously found  
21 to rapidly induce a unique endocytosis which can leak substances with molecular weights <70,000  
22 (Hasan et al., 2016; Torao et al., 2020). It is considered that the IP-delivered ODN could be taken up  
23 via the unique endocytosis and delivered in the cytoplasm of skin cells before degradation in the skin  
24 tissue. In addition, our previous reports demonstrated cytoplasmic delivery of siRNA via weak  
25 electric current treatment without loss of the activity of siRNA in *in vitro* (Hasan et al., 2016; Hasan

1 et al., 2019). Based on these findings, it is suggested that the IP treatment should not affect the ODN  
2 stability.

3 In the present study, we demonstrated efficient intradermal delivery of NF- $\kappa$ B decoy ODN  
4 by overcoming the thickened pathological skin barrier via synergistic effects of IP and AT1002  
5 analog pretreatment, and successfully achieved treatment of psoriasis. The high costs and undesirable  
6 adverse side effects (resulting from frequent administrations) associated with nucleic acid  
7 therapeutics are major challenges for their use in the treatment of diseases (Brezinski et al., 2015;  
8 Miller and Pisani, 1999). In this study, single administration of NF- $\kappa$ B decoy ODN by the  
9 combination IP system was shown to effectively decrease mRNA levels of inflammatory cytokines  
10 and ameliorate psoriasis symptoms in IMQ-treated model rats. Hence, IP combined with the AT1002  
11 analog is expected to realize non-invasive and efficient intradermal delivery of nucleic acid  
12 therapeutics and reduce dosage and frequency of administration, which may lead to improvement of  
13 quality of life in patients suffering from psoriasis. For transdermal delivery of hydrophilic  
14 macromolecules including nucleic acid therapeutics, low bioavailability is known as one of the  
15 serious problems (Levin et al., 2005; Seong et al., 2017). Since combination of pretreatment with  
16 AT1002 analog and NF- $\kappa$ B decoy ODN could enhance transdermal permeation of IP-administered  
17 ODN and its therapeutic efficacy in psoriasis model rats, the combination IP system employed in the  
18 present study is considered to increase the bioavailability of ODN after IP treatment compared with  
19 IP alone. Although we used NF- $\kappa$ B decoy ODN as a representative nucleic acid therapeutic in the  
20 present study, we previously demonstrated successful delivery of other macromolecular drugs, such  
21 as antibodies, siRNA, etc. Results of the present study suggest that application of a combination IP  
22 system with the AT1002 analog can increase the therapeutic efficacy of such macromolecular drugs.

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1 **5. Conclusions**

2 In summary, results of the present study demonstrate the utility of a combination of IP and  
3 the tight junction-opening peptide AT1002 to overcome the thickened psoriatic skin barrier to enable  
4 efficient intradermal delivery of nucleic acid therapeutics for the treatment of psoriasis. Pretreatment  
5 of skin with IP-administered AT1002 analog could enhance transdermal delivery of FAM-ODN via  
6 IP. Moreover, the delivered ODN broadly extended from the epidermis to the dermis layers of  
7 psoriatic skin; although FAM-ODN was found to distribute on the surface of the epidermis in the  
8 group receiving IP alone. Intradermal administration of NF- $\kappa$ B decoy ODN via IP combined with  
9 AT1002 analog pretreatment significantly suppressed IMQ-induced upregulation of mRNA levels of  
10 TNF- $\alpha$  and IL-6, which cytokines are related to pathological progression of psoriasis. Moreover,  
11 NF- $\kappa$ B decoy ODN delivered via IP combined with the AT1002 analog significantly ameliorated  
12 epidermis hyperplasia in psoriasis model rats. Taken together, these results suggest that combination  
13 of IP with the AT1002 analog could synergistically affect the state of the thickened psoriatic skin  
14 barrier to achieve transdermal delivery of NF- $\kappa$ B ODN into the inflamed skin, and that intradermal  
15 delivery of NF- $\kappa$ B decoy ODN by the combination IP system could be useful for the treatment of  
16 psoriasis.

17

18

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22

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24 **Declaration of interest statement**

25 The authors declare no competing financial interests.

26

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14

15

1 **Figure legends**

2

3 Fig. 1. Intradermal distribution of IP-administered fluorescence-labeled oligodeoxynucleotides in  
4 healthy and psoriatic skin

5 Images of dorsal skin of healthy (A) and IMQ-treated psoriasis model rats (B) stained with  
6 HE. Stratum corneum, epidermis, and dermis layers are indicated. Confocal images of frozen skin  
7 sections (10  $\mu\text{m}$ ) of rats topically applied with FAM-ODN (IP (-)) for 1 h (C) and immediately after  
8 treatment by IP (0.34 mA for 1 h) with PBS (D). FAM-ODN was transdermally administered into  
9 healthy (E) or IMQ-treated psoriasis model rats (F) via IP. Immediately after IP, FAM fluorescence  
10 was observed with a confocal microscope (C; FAM-ODN (IP (-)), D; PBS IP (+), E; FAM-ODN IP  
11 (+) in healthy rats, F; FAM-ODN IP (+) in psoriasis model rats). Scale bars = 100  $\mu\text{m}$ . Experiments  
12 were independently performed three times, and each experiment showed similar profiles.

13

14 Fig. 2. Intradermal distribution of NF- $\kappa$ B decoy ODN in thickened psoriatic skin delivered via IP  
15 combined with the AT1002 analog

16 FAM-ODN IP and pretreatment with AT1002 analog IP were performed for healthy rats as  
17 shown in the experimental schedule (A). Immediately after IP, FAM fluorescence was observed in  
18 the skin of the group receiving IP alone (B), IP combined with the control 10-mer peptide (C), and IP  
19 combined with the AT1002 analog pretreatment group (D). Average delivery depths of FAM-ODN  
20 from the skin surface of healthy rats (E). The psoriasis model rats were prepared by topical  
21 application of IMQ cream (60 mg/rat/treatment) for a total of four times. At 24 h after the 4<sup>th</sup> IMQ  
22 treatment, each IP was performed, followed by preparation of frozen skin sections (10  $\mu\text{m}$ )  
23 immediately after 1-h IP (F). Confocal images of FAM-ODN IP alone (G), IP combined with the  
24 control 10-mer peptide (H), and FAM-ODN IP combined with AT1002 analog pretreatment (I).  
25 Average delivery depths of FAM-ODN from the psoriatic skin surface (J). Scale bars = 100  $\mu\text{m}$ . Data  
26 are mean  $\pm$  S.D. (n=3). \*\*  $P < 0.01$ , \*\*\*  $P < 0.001$ .

1 Fig. 3. Intradermal distribution of fluorescence-labeled AT1002 analog administered via IP in healthy  
2 and psoriasis model rats.

3 Healthy (A: 0 h after 1-h IP, B: 2 h after 1-h IP) and IMQ-treated psoriasis model (24 h after  
4 4<sup>th</sup> IMQ treatment; C: 0 h after 1-h IP, D: 2 h after 1-h IP) rats were transdermally FITC-labeled  
5 AT1002 analog by IP (0.34 mA for 1 h). At 0 or 2 h after 1-h IP, frozen skin sections (10  $\mu$ m) were  
6 prepared, and the FITC fluorescence in skins were observed by confocal laser scanning microscopy.  
7 Scale bars = 100  $\mu$ m.

8

9 Fig. 4. Effects of NF- $\kappa$ B decoy ODN delivered by a combination of IP and AT1002 analog  
10 pretreatment on inflammatory cytokine mRNA levels.

11 IMQ-treated psoriasis model rats were transdermally administered NF- $\kappa$ B decoy ODN (50  
12  $\mu$ g dose/rat) or PBS by IP (0.34 mA for 1 h) at 24 h after the 4<sup>th</sup> IMQ treatment (A). For the group  
13 receiving IP combined with the AT1002 analog, pretreatment with IP of the AT1002 analog (400  $\mu$ g  
14 AT1002 dose; 0.34 mA for 1 h) was performed 3 h prior to the start of ODN administration.  
15 Twenty-four hours after IP of NF- $\kappa$ B decoy ODN, mRNA levels of TNF- $\alpha$  (B) and IL-6 (C) were  
16 evaluated. The relative transcript levels (%) of TNF- $\alpha$  and IL-6 in each group to those in the  
17 untreated group (IMQ (-)) are shown. Data are mean  $\pm$  S.D. (n=4). \*  $P$ <0.05, \*\*  $P$ <0.01.

18

19 Fig. 5. Amelioration of epidermis hyperplasia in psoriasis model rats by NF- $\kappa$ B decoy ODN  
20 delivered via IP combined with AT1002 analog pretreatment.

21 IP administration of NF- $\kappa$ B decoy ODN (50  $\mu$ g dose/rat) and pretreatment with AT1002  
22 analog (400  $\mu$ g dose as AT1002) IP were performed as shown in Fig. 3A. At 24 h after IP of NF- $\kappa$ B  
23 decoy ODN, the 10- $\mu$ m frozen skin sections were prepared and stained with HE. Images of skin  
24 sections from untreated (A; n=3), IMQ-treated psoriasis model rats (B; n=3), and psoriasis model rats  
25 treated with NF- $\kappa$ B decoy IP alone (C; n=3) or combined with AT1002 analog pretreatment (D; n=3).  
26 Scale bars = 100  $\mu$ m. The average epidermis layer thickness of each group of rats was measured

1 from >20 images of HE-stained skin sections per rat (E). Data are mean  $\pm$  S.D. (n=3). \*\*  $P < 0.01$ .

2

3 Table 1. Primer sequences for real-time RT-PCR.

Gene	Forward (5' to 3')	Reverse (5' to 3')
TNF- $\alpha$	CGTAGCAAACCACCAAGCA	CGTAGCAAACCACCAAGCA
IL-6	TCCTACCCCAACTTCCAATGCTC	TTGGATGGTCTTGGTCCTTAGCC
GAPDH	CCCCAATGTATCCGTTGTG	TAGCCAGGATGCCCTTTAGT

4

5

6

Fig. 1

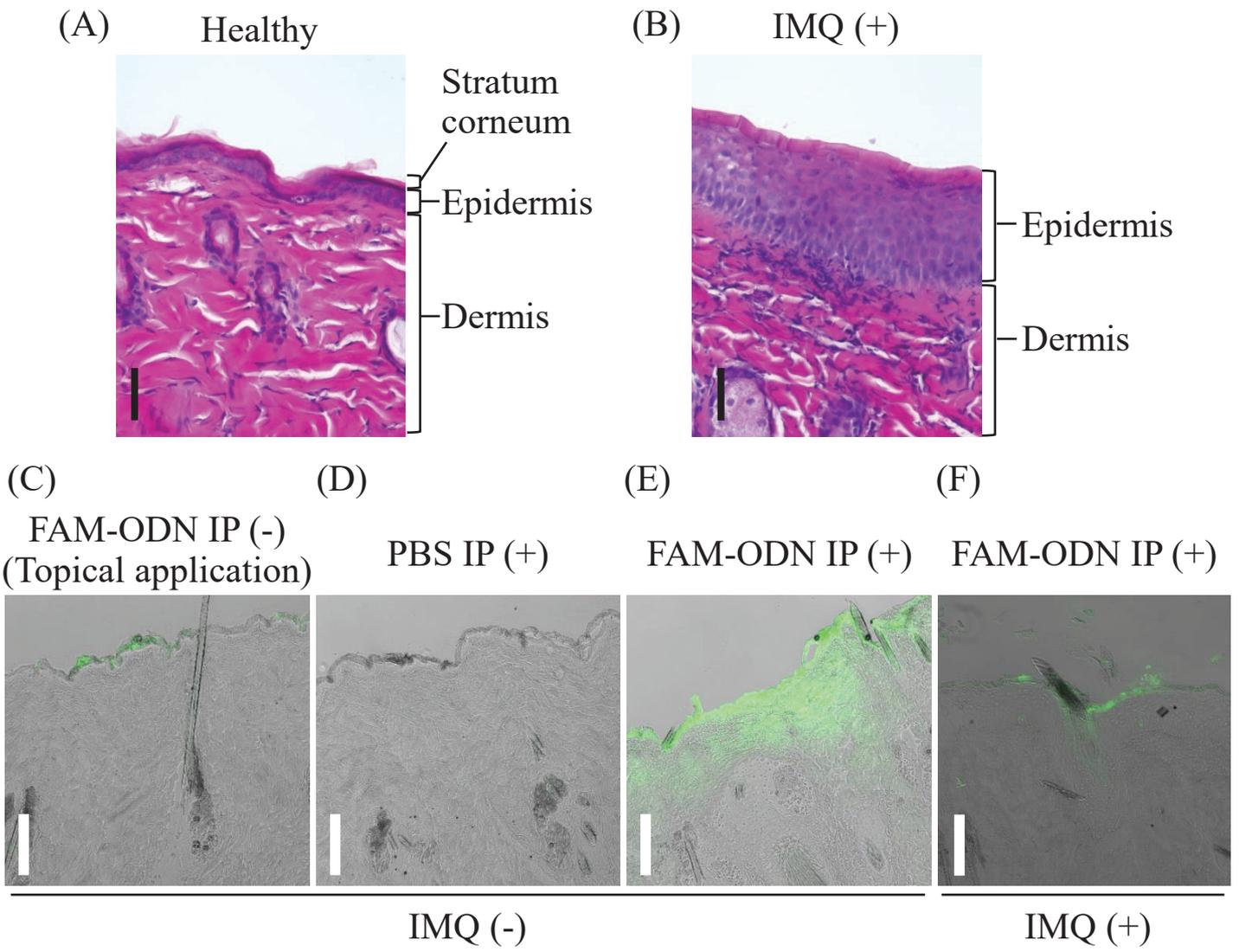
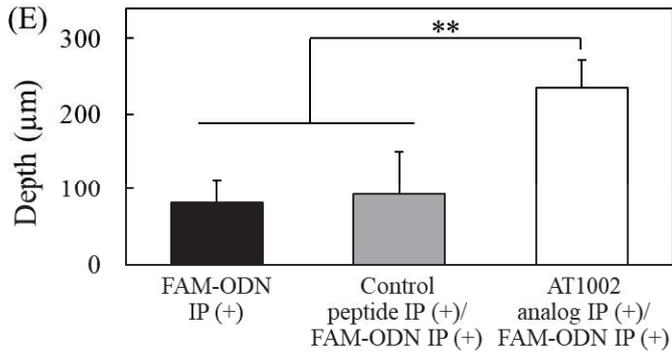
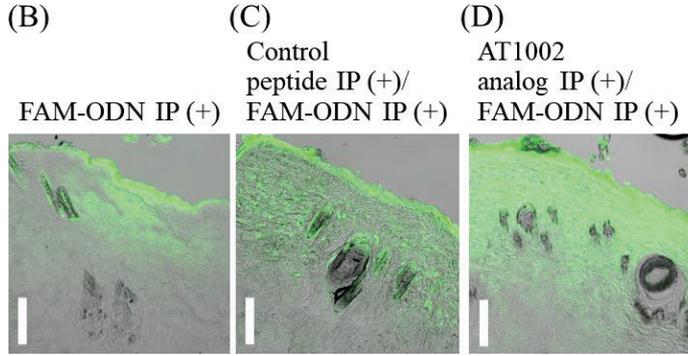
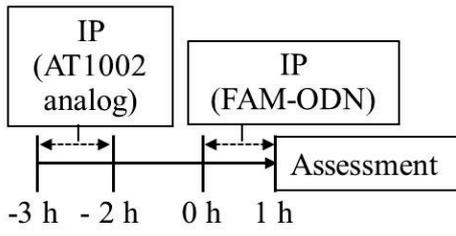


Fig. 2

(A) Healthy rats



(F) Psoriasis model rats

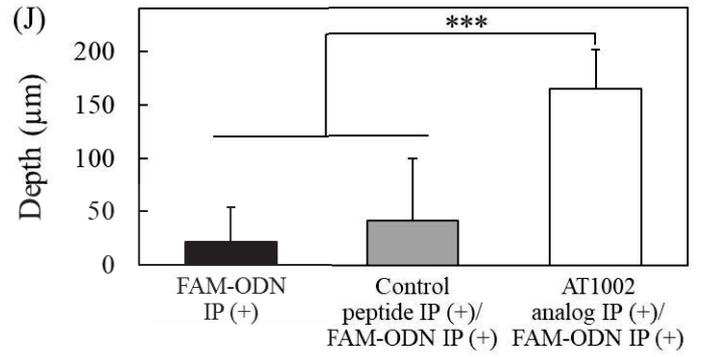
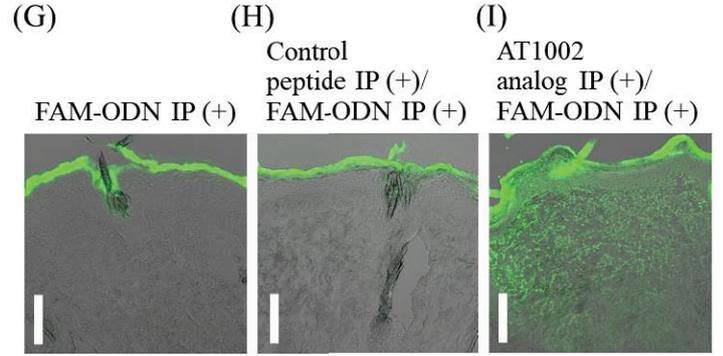
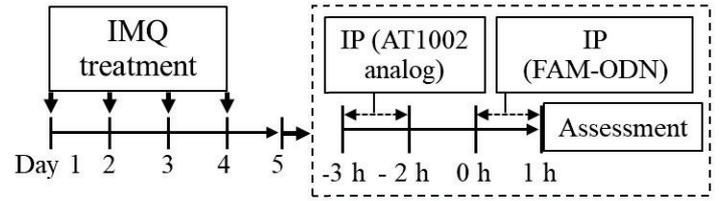


Fig. 3

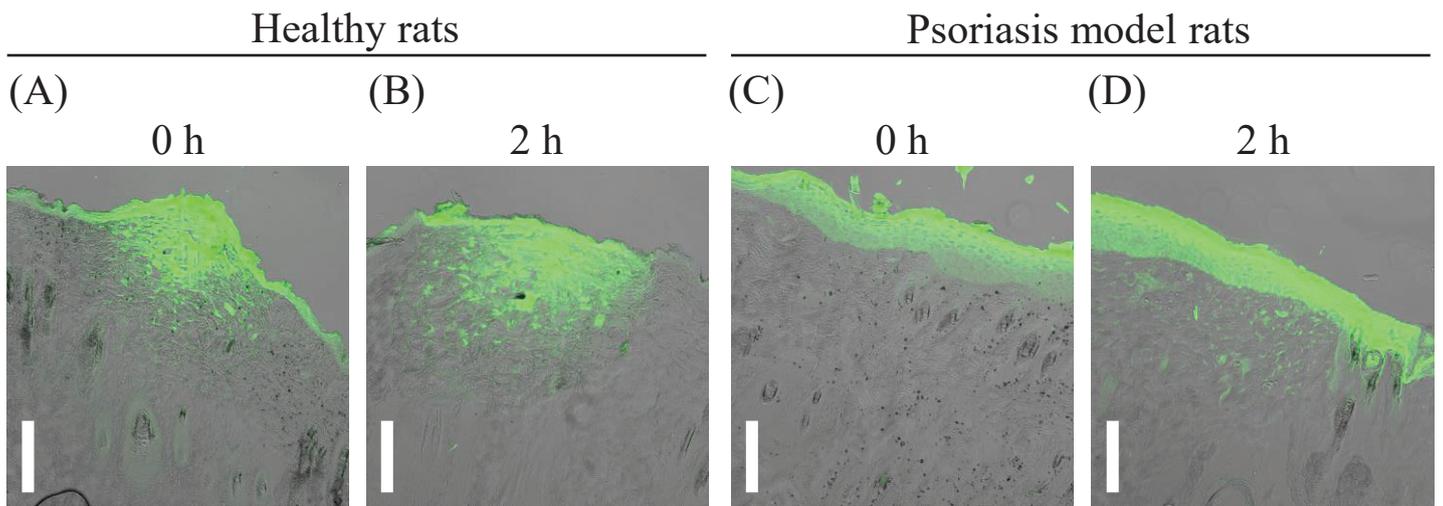
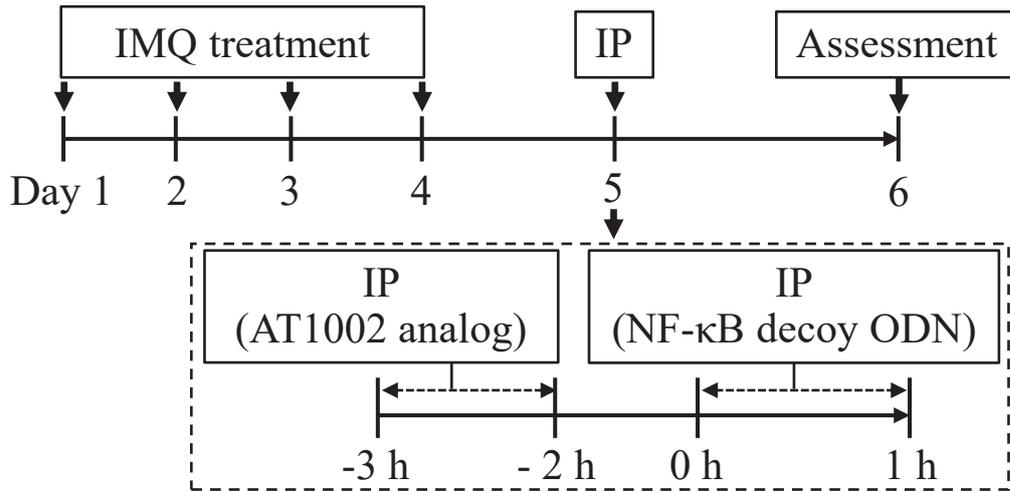
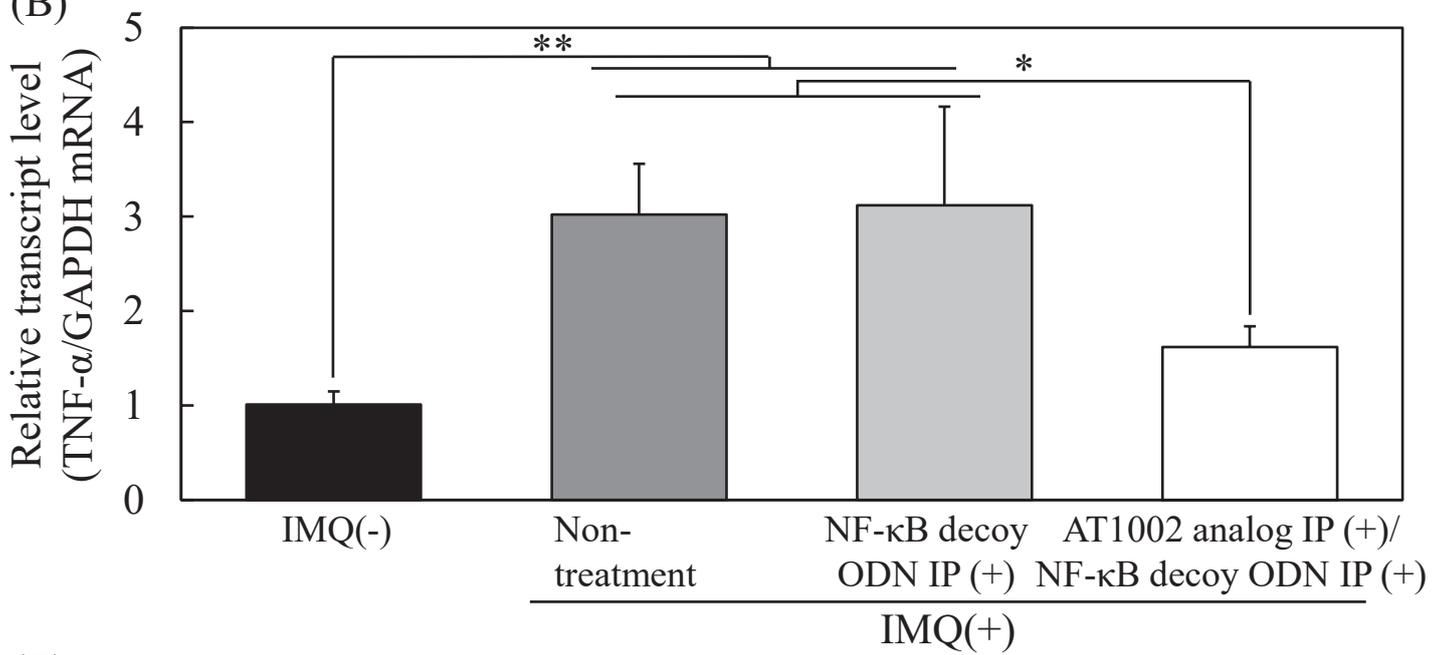


Fig. 4

(A)



(B)



(C)

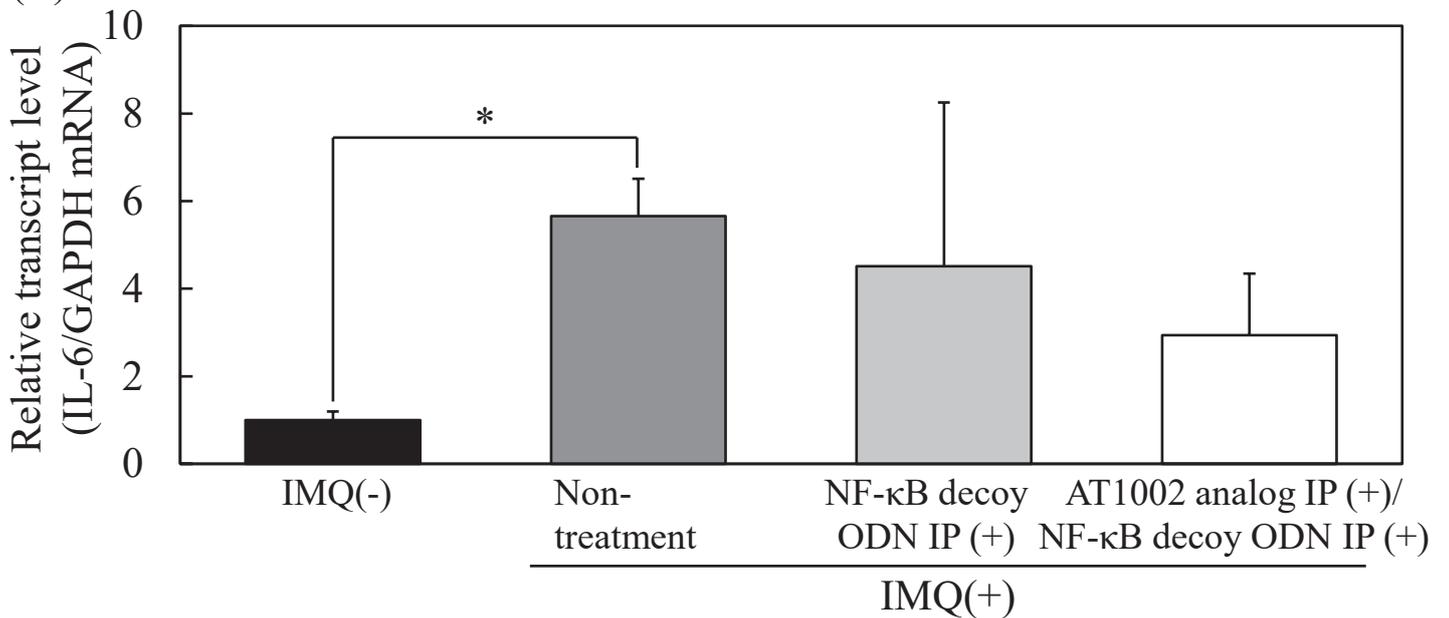


Fig. 5

IMQ(+)

